

Distinct cortical systems reinstate the content and context of episodic memories

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Running title: Content and context reinstatement

1 **Abstract**

2 Episodic recall depends upon the reinstatement of cortical activity present during the formation of a memory. We
3 identified dissociable cortical networks via functional connectivity that uniquely reinstated semantic content and
4 temporal context of previously studied stimuli during free recall. Network-specific reinstatement predicted the
5 temporal and semantic organization of recall sequences, demonstrating how specialized cortical systems enable the
6 human brain to target specific memories.

7 Introduction

8 Episodic recall allows us to remember the past, bringing back memories from a specific place or time. This
9 type of memory retrieval involves the reinstatement of encoding-related neuronal activity that codes for memory
10 attributes¹ (e.g., a specific person² or place³). Neural reinstatement has been proposed as a mechanism for targeting
11 individual memories during memory search^{4,5}, and subsequent studies have demonstrated content^{2,6,7} and context^{3,8}
12 reinstatement preceding memory recall. Thus, these two types of reinstatement may serve to target memories that
13 contain certain content or are placed in specific contexts. However, because studies typically focus on either content
14 or context reinstatement in isolation, we know relatively little about how these types of information reinstate across
15 the brain.

16 Consistent with the longstanding distinction between episodic and semantic memory⁹ neuroimaging and
17 electrophysiological studies suggest that separable cortical systems support memory for the semantic meaning and the
18 spatiotemporal context of experienced events¹⁰⁻¹⁴. Specifically, researchers have identified a posterior medial (PM)
19 network of regions, including parahippocampal, retrosplenial, and posterior parietal cortices, that activates during the
20 processing of contextual information^{15,16}. By contrast, other work has identified an anterior temporal (AT) network
21 of regions that appears critical for semantic and conceptual memory^{17,18}. This network includes the ventral temporal
22 pole and perirhinal cortices¹⁹. Because these two networks interact with the hippocampus during memory formation
23 and retrieval^{14,20}, we predicted reinstatement within these two systems would reflect either the content or context of
24 retrieved memories.

25 Neuroimaging studies that measure population-level neuronal activity have demonstrated reinstatement across cortical
26 systems during memory retrieval. For example, content-related patterns of spectral power from intracranial
27 electroencephalography (iEEG) across prefrontal and temporal cortices reinstate prior to memory recall^{6,21}.
28 Slowly-changing patterns of iEEG power in the temporal lobe, consistent with a representation of temporal context⁵,
29 reinstate during retrieval and account for temporal organization of recall sequences⁸. Functional MRI studies,
30 which provide greater sampling of cortical systems than invasive recording techniques, have demonstrated contextual
31 reinstatement within the hippocampus²² and functionally connected PM regions²³. Multiple regions within the PM
32 network, including the angular gyrus and medial prefrontal cortex, reinstate event-specific patterns of activity²⁴,

33 suggesting this network may be involved in representing the content of memories within a specific episodic context.
34 It is possible that these findings stem from representations of content and context integrated within a single cortical
35 system, coding the full range of attributes in memory. In contrast, the PM and AT networks may independently drive
36 hippocampal-dependent retrieval, serving as distinct cortical pathways to recall.

37 To examine the contributions of cortico-hippocampal networks to recall behavior, we utilized a computational
38 modeling technique originally developed to predict patterns of brain activity based on the semantic content of
39 individual stimuli^{25–27}. This method takes advantage of the sensitivity of neural signals to semantic attributes of
40 presented items. By learning how activity in the brain is shaped by semantic attributes, these models can reliably
41 decode the semantic content of stimuli from an observed pattern of brain activity. We extended this technique to
42 develop context-based models that were trained to predict patterns of brain activity based on the temporal context
43 (i.e., at which point in time in the experiment) in which stimuli were presented. By applying these models to iEEG
44 signals recorded while subjects performed a free-recall task, we tested whether content- and context-based memory
45 representations are reinstated within distinct cortical systems: the AT and PM networks.

46 **Results**

47 We recorded iEEG from neurosurgical patients ($n = 69$) while they performed a free-recall task with items drawn
48 from 25 distinct categories presented in same-category pairs (Fig. 1a). Patients recalled an average of 31% (0.02
49 SEM) of list items. Both the serial position and category of items influenced their probability of recall. We observed
50 a primacy effect, as evidenced by a recall advantage for items presented in the first (mean 49%, 0.03 SEM; $t_{68} =$
51 $9.2, P < 0.0001$) and second (mean 38%, 0.03 SEM; $t_{68} = 4.9, P < 0.0001$) serial positions (Fig. 1b). To evaluate
52 category-level differences in recall performance, we compared the proportion of items recalled from each category to
53 the average across all items (Fig. 1c). We found patients had better memory for zoo animals (mean 42%, 0.03 SEM;
54 $t_{68} = 4.1, P = 0.0001$) and weather (mean 39%, 0.02 SEM; $t_{68} = 3.3, P = 0.001$), and worse memory for electronics
55 (mean 22%, 0.02 SEM; $t_{68} = -4.4, P < 0.0001$).

56 In addition to overall recall performance, the serial position and category of items influenced the order in which items
57 were recalled. Recall clustering (e.g., consecutively recalling same-category items) indicates that the retrieval cue

58 used during memory search targets certain properties of the studied items. Because no retrieval cues are provided to
59 the subject during free recall, the cue must be internally generated by reinstatement of information present during the
60 study period. To examine category clustering, we used a word embedding model²⁸ to derive a vector representation
61 of each studied item. To illustrate the similarity structure derived from the word2vec model, we projected the
62 300-dimensional word representations onto a three-dimensional space derived using principal component analysis
63 (Fig. 1d). We measured clustering with temporal and categorical factor scores, which indicate whether clustering
64 is above or below chance levels²⁹(see Fig. 1e for example measures). Recall sequences exhibited both categorical
65 ($t_{68} = 30.7, P < 0.0001$) and temporal ($t_{68} = 10.8, P < 0.0001$) clustering (Fig. 1f). These clustering effects remained
66 after accounting for potential confounds due to the list structure (see Methods). Adjusted measures of categorical
67 ($t_{68} = 25.6, P < 0.0001$) and temporal ($t_{68} = 11.4, P < 0.0001$) clustering also indicated significant levels of recall
68 organization (Supplementary Fig. 2). Both recall performance and clustering demonstrated reinstatement of both
69 semantic content and temporal context occurred during memory search.

70 *PM and AT networks contain representations of context and content during encoding*

71 To assess representations of temporal context and semantic content within PM and AT networks, we first defined these
72 networks based on an independent resting-state fMRI analysis (Fig. 2a; see Methods for details)³⁰. This analysis
73 follows the standard method of correlating the BOLD timeseries between a region of interest and other regions
74 distributed throughout the rest of the brain³¹. Regions with connectivity to temporal polar cortex defined the AT
75 network. These regions included inferior lateral prefrontal cortex, anterior temporal cortex, and inferior angular gyrus
76 (Fig. 2a, green). Regions with connectivity to the posterior angular gyrus defined the PM network (Fig. 2a, purple).
77 Cortical regions within this network included the posterior cingulate cortex, precuneus, parahippocampal cortex, and
78 posterior parietal cortex (see Supplementary Fig. 1 for details regarding electrode coverage).

79 Synchronous low-frequency activity across the brain signals memory processing³², with theta oscillations responsible
80 for interactions between hippocampus and cortex during memory search³³. Prominent theories propose synchronous
81 interactions coordinate network communication³⁴, which would support hippocampal-dependent reinstatement of
82 memory content. Thus, we predicted synchronous activity in both PM and AT networks during the free-recall task.
83 We next tested the hypothesis that PM and AT networks defined by resting-state fMRI would predict correlations

84 in low-frequency power during task performance. Previous work has established correspondence between networks
85 defined by resting-state fMRI and iEEG^{35,36}. However, it is possible that different network structures emerged in iEEG
86 signals during the recall task. For example, these two cortical systems could reconfigure into a single network. We
87 predicted distinct networks to emerge as subjects perform the task, supporting the hypothesis that separable cortical
88 systems are involved in the representation of content and context.

89 To examine the separability of PM and AT networks, we asked whether theta exhibited greater connectivity within than
90 between the two networks. We measured connectivity by correlating spectral power across trials of the free-recall task.
91 Such trial-by-trial variability in power reflects endogenous fluctuations across neural networks^{35,37,38}. Because these
92 estimates of connectivity can be spuriously elevated due to proximity of recording sites³⁶ (see Fig. 3 for evidence
93 of drop off in connectivity with inter-electrode distance), we used a bootstrap matching procedure to control for
94 differences in distance between contacts located within the same network or across both networks (see Methods).
95 Using this approach, low-frequency power was significantly more correlated within the AT network than between the
96 PM and AT network (Fig. 2a). This effect held at the lower (3 Hz, $t(64) = 4.97, P < 0.0001$), intermediate (5 Hz,
97 $t(64) = 3.67, P < 0.0001$), and upper range of theta (10 Hz, $t(64) = 3.12, P < 0.0001$). Within the PM network, we
98 found evidence for synchronous activity near the upper end of theta (10 Hz, $t(64) = 2.13, P = 0.04$). We also explored
99 whether network-specific coupling occurred at higher frequencies, spanning beta and gamma ranges. We did not
100 identify any higher frequency effects within the AT network. Coupling in the low beta range was enhanced within the
101 PM network (17 Hz, $t(64) = 2.70, P = 0.009$). These results show that changes in spectral power were coherent within
102 each of these two networks, consistent with their identification as dissociable networks from resting-state fMRI.

103 Having validated the PM and AT networks in our iEEG recordings, we next sought to evaluate their respective roles in
104 the reinstatement of memories' semantic content and temporal context. To do this, we trained multivariate models to
105 predict brain activity based on the semantic content and temporal context of items presented at encoding. We modeled
106 changes in spectral power from 3 to 180 Hz at each recording site from either the content- or context-based attributes of
107 each item (Fig. 2b). Using these models, we predicted the pattern of spectral power for each serial position or category.
108 We compared these predictions to held-out items in a cross-validation procedure that tested whether it was possible to
109 decode either the serial position or category from brain activity observed within a given network. In addition, applying

110 these models to patterns of spectral power during memory search allowed us to compare reinstatement across the two
111 networks.

112 We assessed each model's decoding performance during the encoding phase of the experiment, as subjects studied
113 list items. We used a bootstrap procedure ($n = 1000$) to estimate decoding performance from five randomly sampled
114 recording sites within each network (this approach allowed us to control for greater electrode coverage in the AT
115 network, see Fig. 1b and Methods for further details). Applying this technique, we reliably decoded the category of
116 items in both the PM (median AUC = 0.54, $Z = 6.9$, $P < 0.0001$) and AT (median AUC = 0.54, $Z = 7.1$, $P <$
117 0.0001) networks (Fig. 2c), but category decoding did not differ between the two networks (median Δ AUC = 0.002,
118 $Z = 0.8$, $P = 0.45$). We also reliably decoded the serial position of items in both the PM (median AUC = 0.71, $Z = 7.2$,
119 $P < 0.0001$) and AT (median AUC = 0.70, $Z = 7.2$, $P < 0.0001$) networks (Fig. 2d). Here, our serial position model
120 achieved more accurate decoding in the PM than in the AT network (median Δ AUC = 0.002, $Z = 2.1$, $P = 0.04$). These
121 bootstrap results provide a lower bound for the true decoding performance for a given network (see Supplementary
122 Fig. 4) and confirm the representation of semantic and temporal information across the PM and AT networks during
123 encoding.

124 *Reinstatement of content and context in PM and AT networks*

125 Having established the ability to decode temporal context (serial position) and semantic content (category) from
126 encoding-period neural activity in the PM and AT networks, we next asked whether these two types of information
127 reinstated during free recall. To measure reinstatement, we tested our category and serial position models on patterns
128 of neural activity in the moments preceding recall (from 900 to 100 msec prior to vocalization, in 20 msec intervals;
129 Fig. 3a). We observed reinstatement of temporal information in the PM network and semantic information in both
130 the PM and AT networks. Temporal context reinstated in the PM network from 600 to 400 msec before overt recall
131 (Fig. 3b, top panel). Content reinstatement was sustained throughout the pre-recall period (Fig. 3b, bottom panel)
132 in both PM and AT networks. Moreover, these two forms of reinstatement differed between the two networks, with
133 greater content reinstatement in the AT network (Fig. 3b; $P < 0.05$, FWER corrected). These findings demonstrate
134 specificity of contextual reinstatement within the PM network. In contrast to previous studies that relied upon similarity
135 in neural activity over time to identify contextual information^{8,22,23,39,40}, we demonstrate the ability to recover the

136 serial position of recalled items from reinstatement in the PM network. We also show greater, sustained content
137 reinstatement within the AT network. These unique patterns of reinstatement reveal a dissociation between content
138 and context reinstatement across the PM and AT networks.

139 Our finding that reinstatement of temporal context is specific to the PM network relies upon chance-level decoding
140 within the AT network. It is possible that by limiting the number of electrodes included in this analysis (which
141 was necessary for comparisons between networks), we impaired our ability to detect reinstatement, particularly if
142 information was represented in a distributed manner. To evaluate this possibility, we examined decoding performance
143 after incorporating additional electrodes into our analysis (Supplementary Fig. 4). Adding electrodes produced more
144 robust category reinstatement effects in both the PM ($\chi^2_1 = 5.7, P = 0.02$) and AT ($\chi^2_1 = 31.4, P < 0.0001$) networks.
145 This analysis also revealed stronger context reinstatement in the PM ($\chi^2_1 = 6.7, P = 0.009$) but not the AT ($\chi^2_1 = 0.8,$
146 $P = 0.36$) network when incorporating additional features. These findings provide additional support for the specificity
147 of context reinstatement to the PM network and suggest that decoding accuracy was limited by anatomical coverage
148 and the spatial resolution of recordings.

149 To rule out the possibility that epileptiform activity influenced our ability to detect reinstatement, we examined whether
150 electrodes that were either within the seizure onset zone, exhibited inter-ictal spiking, or located near pathological
151 tissue impacted decoding performance. We repeated our decoding analyses after excluding these electrodes and found
152 a remarkably similar pattern of results (Supplementary Fig. 5). We found no evidence that signals from these electrodes
153 impacted our ability to decode information at encoding (all $\chi^2_1 < 0.25, P's > 0.61$) or recall (all $\chi^2_1 < 0.43, P's > 0.53$).
154 As such, reinstatement reflected changes in spectral content associated with physiologically and cognitively normal
155 processes.

156 Cortical reinstatement has been shown to predict how memory search unfolds^{4,21}, with cortical representations
157 providing a top-down cue for the memory system to retrieve specific information. As such, it is possible that the
158 PM and AT networks are responsible for targeting stored memories with specific content- or context-based attributes.
159 To test this hypothesis, we examined whether differences in reinstatement across the two networks predicted the
160 tendency of subjects to organize their recall sequences along temporal or categorical dimensions. Consistent with prior
161 work linking cortical reinstatement to memory organization^{6,8}, variability in the organization of a subject's memory

162 was predicted by cortical reinstatement during memory search (Fig. 3c). Greater reinstatement of context-based
163 representations within the PM network tracked the tendency to consecutively recall items from nearby serial positions
164 ($r_{67} = 0.26$, $P = 0.028$). Increased reinstatement within the AT network was associated with greater organization
165 based on the categorical structure of the list ($r_{67} = -0.35$, $P = 0.003$). Representations encoded in these two cortical
166 systems can differentially guide memory search, biasing how and what we remember.

167 **Discussion**

168 We report evidence that the reinstatement of content- and context-based information occurs within distinct cortical
169 networks. Furthermore, the quality of reinstatement within a given network was predictive of a subject's tendency
170 to organize their memories along either temporal or categorical dimensions. These results help resolve conflicting
171 viewpoints on how distinct neural representations contribute to memory search. Episodic retrieval occurs when a
172 memory cue converges on the hippocampal formation, prompting associative recall⁴¹. Multiple cortical structures
173 have been proposed to represent temporal context, which cues episodic recall⁴², including lateral prefrontal cortex⁵
174 and parahippocampal inputs to the hippocampus⁴³. Despite evidence implicating these structures in representing
175 temporal information^{8,22,44-47}, it has been unclear whether these brain regions are the primary drivers of episodic
176 recall. Our findings of greater reinstatement of context within the PM network and content within the AT network
177 resolve this ambiguity by characterizing the contributions of these cortico-hippocampal networks to memory search.

178 Our findings complement previous studies of the neural bases of memory search^{6,8,21} that have linked neural
179 reinstatement to the organization of human memory. Along with fMRI investigations of temporal coding in the MTL
180 and cortico-hippocampal networks^{22,23}, these previous studies identified candidate regions for the representation of
181 temporal context based on slow changes in the similarity of neural patterns over time. Here, our modeling approach
182 enabled us to recover the temporal position of items within each list, irrespective of the list in which the item was
183 encoded. This rules out the possibility that context-like signals emerge from the covert retrieval or maintenance of
184 list items throughout study lists, an inherent limitation of prior work. Given the PM network specifically reinstates
185 contextual codes that predict the temporal organization of recall sequences, it is likely that this network is necessary
186 to target memories from specific episodic contexts. Because the present findings are inherently correlational in nature,
187 future studies could provide causal evidence between network reinstatement and recall organization via noninvasive

188 or direct electrical stimulation. Adaptation of recently developed closed-loop stimulation techniques^{48,49} may allow
189 stimulation during memory search to bias recall of information from a specific context.

190 Unlike reinstatement of contextual information that was specific to the PM network, we were able to decode the
191 category of recalled items from patterns of activity in both networks. Converging evidence from fMRI studies
192 suggests that regions within this network⁵⁰, including the angular gyrus²⁴, represent recollected content in an episode-
193 specific manner. Our findings suggest that temporal coding may be a unique feature of this network, in contrast to
194 representations coded in the AT network. Understanding the nature of these temporal representations, including where
195 they originate and how they are integrated with other forms of episodic information remains to be determined.

196 Our ability to decode the content and context of items in memory reflects multiple neuronal processes. Specifically,
197 the measures of spectral power we examined reflect a combination of broadband and oscillatory processes, including
198 slower (2-4 Hz) and faster (5-10 Hz) theta rhythms that predominate hippocampal networks⁵¹. Broadband shifts in
199 power indicate when memory processing occurs, including concurrent decreases in low frequency and increases in
200 high frequency content⁵²⁻⁵⁴. These broadband shifts are associated with changes in neuronal excitability and correlate
201 with firing rates of locally recorded neurons^{55,56}. Thus, increases in neuronal firing within attribute-specific cortical
202 regions would support accurate decoding. At the same time, reduction of oscillations and increased asynchronous
203 activity supports information coding within cortex^{57,58}. Changes in the amplitude of narrowband oscillations would
204 therefore contribute to decoding performance, at timescales constrained by the speed of the oscillation. Understanding
205 the relative contributions of oscillatory and broadband signals to memory reinstatement remains an important question
206 for future research.

207 Neural models of memory search have suggested that an internal representation of context serves as the primary
208 cue for hippocampal-dependent recall⁵. Our findings argue for an alternative account regarding the neural basis
209 of memory search. One possibility is that semantic representations within the AT system can cue memories in
210 a context-independent manner, prompting recall of memories with similar semantic attributes. If content-based
211 representations can guide memory search in this fashion, one would expect individuals to organize their memories
212 based on semantic content, rather than the temporal order in which it was learned. Indeed, subjects who showed
213 greater reinstatement in the AT network exhibited greater semantic and less temporal organization. This hypothesis

214 is further supported by evidence that content-based activity in the inferior temporal cortex can be used as a top-down
215 signal to bias retrieval to targeted memories⁷. Along these lines, the contextual information represented across the PM
216 network focuses retrieval to a specific temporal context. The effects observed here may reflect a general property of
217 memory search, wherein cortical reinstatement serves as a mechanism to target memories based on network-specific
218 representations.

219 **Methods**

220 *Participants*

221 69 patients (40 male; see Supplementary Table 1 for details) with medication-resistant epilepsy underwent
222 neurosurgical procedures to implant intracranial electrodes (subdural, depth, or both) to determine epileptogenic
223 regions. Data were collected at Dartmouth-Hitchcock Medical Center (Hanover, NH), Emory University Hospital
224 (Atlanta, Georgia), Hospital of the University of Pennsylvania (Philadelphia, PA), Mayo Clinic (Rochester, MN),
225 Thomas Jefferson University Hospital (Philadelphia, PA), Columbia University Medical Center (New York, NY), and
226 University of Texas Southwestern Medical Center (Dallas, TX). Prior to data collection, the research protocol was
227 approved by the institutional review board at each hospital. Informed consent was obtained from either the participant
228 or their guardians.

229 *Free-recall task*

230 Each subject performed a categorized free-recall task in which they studied a list of words with the intention to commit
231 the items to memory. The task was performed at the bedside on a laptop, using PyEPL software⁵⁹. Analog pulses were
232 sent to available recording channels to enable alignment of experimental events with the recorded iEEG signal. Word
233 presentation lasted for a duration of 1600 ms, followed by a blank inter-stimulus interval (ISI) of 750 to 1000 ms (see
234 Fig. 1a). Each list contained items from three distinct categories (four items per category), with two same-category
235 items presented consecutively. The total word pool consisted of 25 distinct categories, with individual items selected
236 as prototypical items within each category⁶⁰. Presentation of word lists was followed by a 20 s post-encoding delay.
237 Subjects performed an arithmetic task during the delay in order to disrupt memory for end-of-list items. Math problems
238 of the form $A+B+C=??$ were presented to the participant, with values of A, B, and C set to random single digit integers.

239 After the delay, a row of asterisks, accompanied by an 800 Hz auditory tone, was presented for a duration of 300 ms
240 to signal the start of the recall period. Subjects were instructed to recall as many words as possible from the most
241 recent list, in any order during the 30 s recall period. Vocal responses were digitally recorded and parsed offline using
242 Penn TotalRecall (<http://memory.psych.upenn.edu/TotalRecall>). Subjects performed up to 25 lists in
243 a single recall session.

244 *Behavioral analysis*

245 To compute behavioral measures of temporal clustering, we used the temporal factor²⁹ score. Temporal factor
246 measures the percentile rank of the absolute lag between successive recalls from the full distribution of available lags
247 for items that have yet to be recalled. To measure category clustering, we computed a category factor which assumes
248 that all items within the same category have a distance of zero and items of different categories have a distance of
249 one. These metrics measure the degree to which recall sequences exhibit organization along temporal or categorical
250 dimensions, with random recall sequences falling at the median of the distribution (i.e., 0.5).

251 We presented same category exemplars in sequential pairs, as in the sequence ($A_1, A_2, B_1, B_2, C_1, C_2, B_3, B_4, \dots,$
252 A_4) where X_i is an exemplar of category X . This list structure creates circumstances where random recall sequences
253 produce factor scores that deviate from the expected value of 0.5. Consider the case where a subject recalls four
254 items from a single category in an arbitrary temporal order. After recalling the first item, the subject could either
255 recall the same-category pair (e.g., A_2 following A_1) or jump to one of the other same-category items (A_3 or A_4).
256 Because more items are available for recall at long temporal lags, sequences generated with random temporal order
257 produce a lower than expected temporal factor score of 0.45. Measures of category clustering can be similarly biased
258 by the list structure. Consider the case where a subject serially recalls four items starting at an arbitrary position in
259 the list, without regard to semantic information. Because same-category pairs are always recalled consecutively, the
260 expected category factor score for these recall sequences is elevated to 0.64. These examples highlight that factor
261 scores can deviate from 0.5 due to the list structure rather than true recall clustering. To rule out this potential
262 confound, we performed a simulation-based control analysis where we generated null distributions from random
263 recall sequences matched to both the number of items recalled and either the temporal or categorical clustering of the
264 observed sequences. We standardized the observed clustering measures based on these null distributions ($n = 1000$),

265 which indicate the amount of clustering expected by chance given the list structure. This analysis is sensitive to
266 clustering that is not confounded by the list structure, such as temporal clustering across category boundaries and
267 category clustering across large temporal lags.

268 *Electrophysiological recordings and data processing*

269 iEEG signal was recorded using subdural grids and strips (contacts spaced 10 mm apart) or depth electrodes (contacts
270 spaced 3-10 mm apart) using recording systems at each clinical site. iEEG systems included DeltaMed & XITek
271 (Natus), Grass Telefactor, and Nihon-Kohden EEG systems. Signals were sampled at 500, 512, 1000, 1024, or
272 2000 Hz, depending on clinical site. Signals recorded at individual contacts were converted to a bipolar montage by
273 computing the difference in signal between adjacent electrode pairs on each strip, grid, and depth electrode. Bipolar
274 signal was notch filtered at 60 Hz with a fourth order 2 Hz stop-band butterworth notch filter in order to remove the
275 effects of line noise on the iEEG signal.

276 *Anatomical localization*

277 Anatomical localization of electrode placement was accomplished using independent processing pipelines for depth
278 and surface electrodes. Post-implant CT images were coregistered with presurgical T1 and T2 weighted structural
279 scans using Advanced Normalization Tools⁶¹. For patients with MTL depth electrodes, hippocampal subfields and
280 MTL cortices were automatically labeled in a pre-implant, T2-weighted MRI using the automatic segmentation of
281 hippocampal subfields multi-atlas segmentation method⁶². Subdural electrodes were localized by reconstructing
282 whole-brain cortical surfaces from pre-implant T1-weighted MRIs using Freesurfer⁶³, and snapping electrode
283 centroids to the cortical surface using an energy minimization algorithm⁶⁴. Reconstructed surfaces were additionally
284 mapped to a population-average surface⁶⁵ that we used to assign network membership based on resting state
285 connectivity of cortical regions defined by a multi-modal cortical parcellation³⁰.

286 *Network assignment and analysis*

287 We assigned recording sites to networks of interest was based on resting state functional connectivity in an independent
288 set of subjects from the Human Connectome Project³⁰. From the Glasser et al. parcellation, we assigned parcels with

289 high connectivity to the posterior angular gyrus (area PGp) to the PM network and parcels with high connectivity to
290 the ventral temporal pole (area TGv) to the AT network. Assignment was based on partial correlations between each
291 parcel and the seed region, to provide a better estimate of direct network connections. Bipolar pairs were assigned
292 to the nearest network if the bipolar centroid was within 8 mm of a parcel within either network, with the exclusion
293 criteria that they could not be within 4 mm of the other network.

294 To evaluate the properties of these two cortical networks, we used a bootstrap sampling procedure to randomly sample
295 from bipolar pairs within each network. In our assessment of functional connectivity, we controlled for the effect
296 of distance between recording sites on functional connectivity. As the distance between recording sites is greater
297 between rather than within functional networks (leading to a biased estimate of connectivity within each network), we
298 controlled the distances within each distribution of connections (i.e., within AT, within PM, or between networks). For
299 each subject, we randomly sampled connections between the two networks. Connections within a given network were
300 sampled without replacement to match the distribution of between network connections by minimizing the differences
301 in connection length. The functional connectivity within and between each network was computed as the Pearson
302 product-moment correlation across encoding events in the experiment. This procedure was repeated 1000 times, and
303 the intrinsic connectivity at a given frequency was estimated from the bootstrap distribution. In circumstances where
304 electrode coverage prevented well matched samples subjects were excluded from analysis ($N = 4$).

305 A similar bootstrap procedure was used to estimate the decoding accuracy of models trained from a given particular
306 network. Networks with greater electrode coverage are likely to have higher decoding accuracy due to the number of
307 features alone. As a result, we randomly sampled five electrodes from each network prior to estimating the ability to
308 decode content and context information from patterns of brain activity. This sampling procedure was repeated 1000
309 times per model evaluation, and the average performance across bootstrap distributions was used to indicate model
310 performance for a given subject.

311 *Spectral power*

312 To compute spectral power during word encoding, we applied the Morlet wavelet transform (wave number 5) to all
313 bipolar electrode EEG signals from the onset to the offset of stimulus presentation, across 8 logarithmically spaced

314 frequencies from 3 to 180 Hz. Spectral power during recall was estimated from 900 ms to 100 ms preceding the
315 onset of response vocalization for correct recalls. Recall events were required to be free of vocalization onsets in
316 the preceding 1500 ms. Power estimates were log transformed and down sampled to 50 Hz. To avoid edge artifacts,
317 we included buffers of 1000 ms surrounding events of interest during the computation of spectral power; mirrored
318 buffering was applied to all retrieval-period data. Prior to modeling, all power estimates were standardized using the
319 mean and standard deviation of each session.

320 *Model fitting and testing*

321 We constructed two models to predict stimulus-related patterns of neural activity as a function of either 1) the
322 taxonomic category of presented stimuli or 2) the serial position of each presented item within the experiment. For the
323 content model, we modeled the neural response as a function of 300 intermediate category features computed using
324 the wrd2vec model²⁸ trained from Google News corpora. Category features were computed by averaging semantic
325 representations across all words presented from a given category. This results in the construction of a high dimensional
326 space that respects the semantic relationships between all of the categories. For the context model, we modeled the
327 neural response to stimuli as a function of serial position within the list, across lists, and across sessions. For subjects
328 in which only a single session was run, the regressor predicting the effect of session on neural activity was excluded.

329 We fit both the content and context models separately to each neural feature (i.e., spectral power at a given frequency
330 and bipolar pair). Ridge regression was used to identify model parameters that minimized prediction error on
331 the training data, which was randomly assigned using a 5-fold cross-validation procedure, holding out individual
332 words. Within each training fold, we performed an additional 10-fold cross-validation procedure (i.e., nested
333 cross-validation⁶⁶) to optimize the regularization coefficient used in each fold. Across the ten folds, we selected
334 the regularization coefficient (from 50 potential parameters log-spaced from 10^{-2} to 10^{10}) that minimized the mean
335 squared error of the model predictions across the training set. The resulting set of model weights across neural
336 features was used to decode either the serial position or category membership for unseen patterns of brain activity. We
337 computed the probability that the observed brain data belonged to each of the 25 categories (or 12 serial positions)
338 by computing the Pearson product-moment correlation between the observed data and the predicted pattern of brain
339 activity for each model. A softmax function was applied to the resultant evidence for each class, and decoding accuracy

340 was measured using area under the receiver operating characteristic curve (AUC) metric across all held out data.

341 To quantify reinstatement effects across each network, we applied models trained to predict patterns of brain activity
342 observed during encoding of words to epochs just prior (from 900 ms to 100 ms before vocalization onset). For each
343 sample within this window, we computed the ability of each model to decode either the category or serial position of
344 recalled words in the validation data. The resulting AUC timeseries were smoothed with with a 7 ms FWHM Gaussian
345 kernel prior to statistical analysis for noise reduction.

346 *Statistics*

347 One-tailed tests were used to assess differences versus chance performance in evaluating decoding accuracy and recall
348 organization. Theoretical chance levels (e.g., an AUC of 0.5 one class vs. all others) were further tested by constructing
349 null distributions via permutation of class labels (i.e., category or serial position).

350 To evaluate the effects of the number of features and potential epileptiform activity on decoding performance, we
351 modeled classifier performance using linear mixed-effects models. Fixed effects included the number of electrodes
352 sampled, and whether the electrode was localized to the seizure onset zone. Intercepts were allowed to vary, treating
353 subject as a random variable. Inference was performed through model comparison using a likelihood ratio test,
354 dropping the effect of interest. Model fits and normality of residuals were confirmed through visual inspection.

355 We corrected for multiple comparisons (across time and frequencies) using a nonparametric permutation procedure.
356 In our analysis of intrinsic connectivity, we performed a nonparametric one sample t test by constructing a null
357 distribution of the maximum t statistic across frequencies, assuming no difference in intrinsic connectivity for
358 connections within and between networks. This assumption was satisfied by random sign flipping of observed values
359 at the subject level. Significance of observed differences in connectivity strength within versus between networks
360 were compared to a distribution constructed from 2000 random permutations, yielding two tailed significance with
361 $P_{FWE} < 0.05$.

362 Multiple comparison correction for network reinstatement followed a similar procedure. We identified significant
363 ($P_{FWE} < 0.05$) clusters in the moments leading up to recall using threshold-free cluster enhancement (TFCE)⁶⁷. The

364 TCFE statistic was computed by taking the original test statistics over the pre-recall period and adjusting by weighting
365 by the height (h) and cluster extent (e):

$$\sum_k h^H e(h_k)^E dh, \quad (1)$$

366 where h_k is one of k cluster forming thresholds ($h_k = h_0, h + dh, \dots, h_{max}$). Height (H) and extent (E) exponents were
367 set to 2 and 0.5 respectively, with the step size in the cluster threshold (dh) set to 0.01. After computing TCFE
368 statistics, we used previously described nonparametric t tests to identify significant clusters based on null distributions
369 ($n = 1000$).

370 Given the limited availability of iEEG data, no statistical methods were used to predetermine sample sizes (number of
371 subjects). The number of trials included in the experiment was determined by practical constraints of patient testing
372 at epilepsy monitoring units. The subjects in this study were a subset of those included in a multi-site collaboration
373 to investigate modulation of human memory via direct electrical stimulation. Subjects with at least 5 recording sites
374 located within both the PM and AT networks who performed categorized free recall were included in the present study.

375 **Data Availability**

376 De-identified data is available at http://memory.psych.upenn.edu/Electrophysiological_Data.

377 **Code Availability**

378 Analysis code for model fitting and evaluation is available at [http://memory.psych.upenn.edu/](http://memory.psych.upenn.edu/Electrophysiological_Data)
379 [Electrophysiological_Data](http://memory.psych.upenn.edu/Electrophysiological_Data).

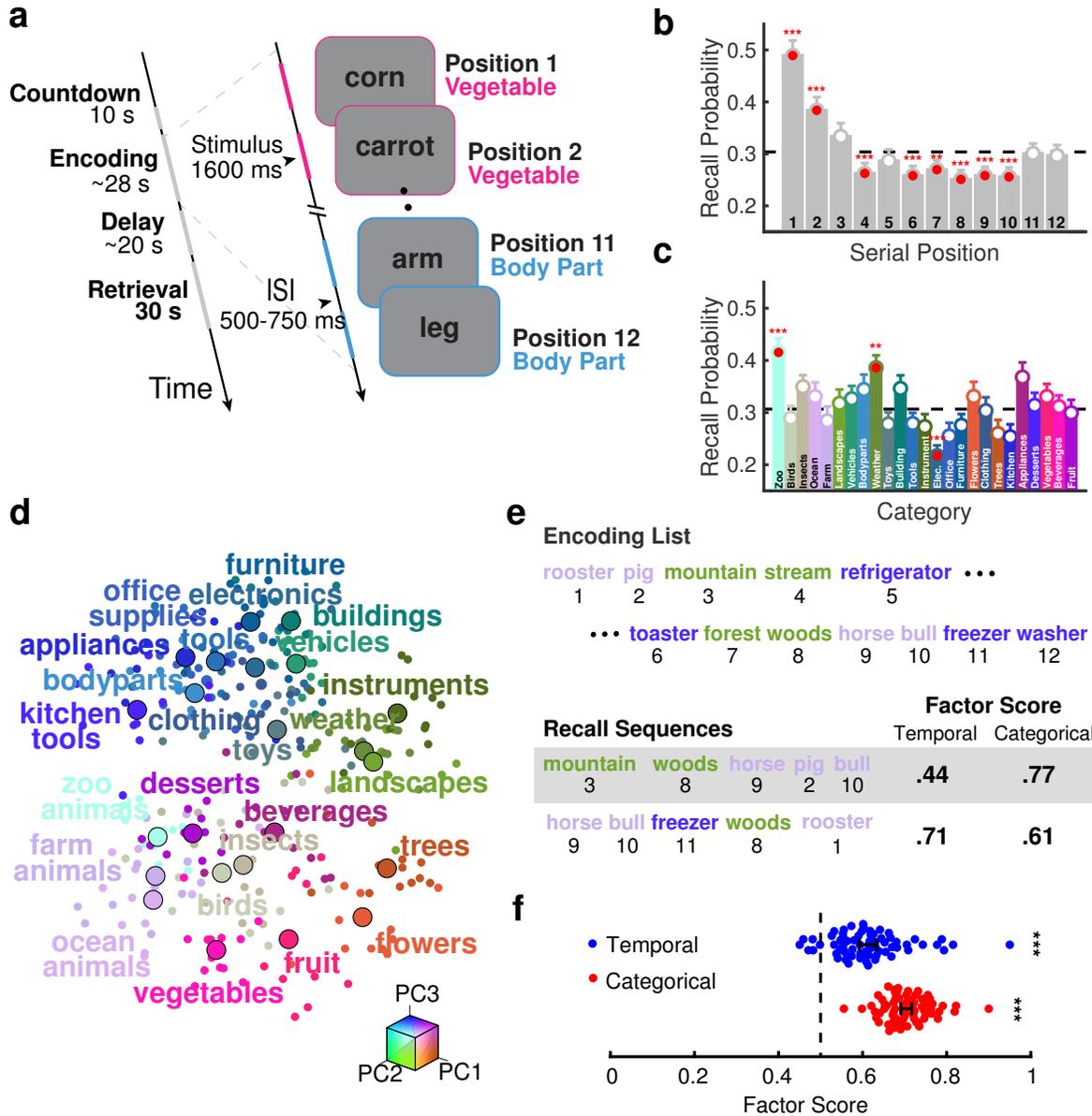


Figure 1 Task and behavioral results. **a**, Schematic of the free-recall task. Left: Task timeline for a single recall trial. Right: List structure and timing during the encoding period. Subjects completed 25 lists per experimental session. **b**, Recall performance by serial position. Significant differences from the mean are indicated. ***, $P < 0.001$; **, $P < 0.01$, FDR corrected. Error bars denote ± 1 SEM. **c**, Recall performance by category. Plotting convention follows panel **b**. **d**, Category representations of stimuli. Each point indicates a word's semantic representation along the first three principal components of the word2vec²⁸ space. Larger points denote the midpoint of all stimuli within a category. Words with similar meaning are spatially proximal. **e**, Factor scores for example recall sequences. Factor scores above 0.5 indicate above chance levels of temporal or categorical organization of recall sequences. **f**, Recall organization. Subjects (indicated by individual points) clustered recalls along temporal and semantic dimensions, as indicated by above chance (dashed line) factor scores. ***, $P < 0.001$. Error bars denote ± 1 SEM.

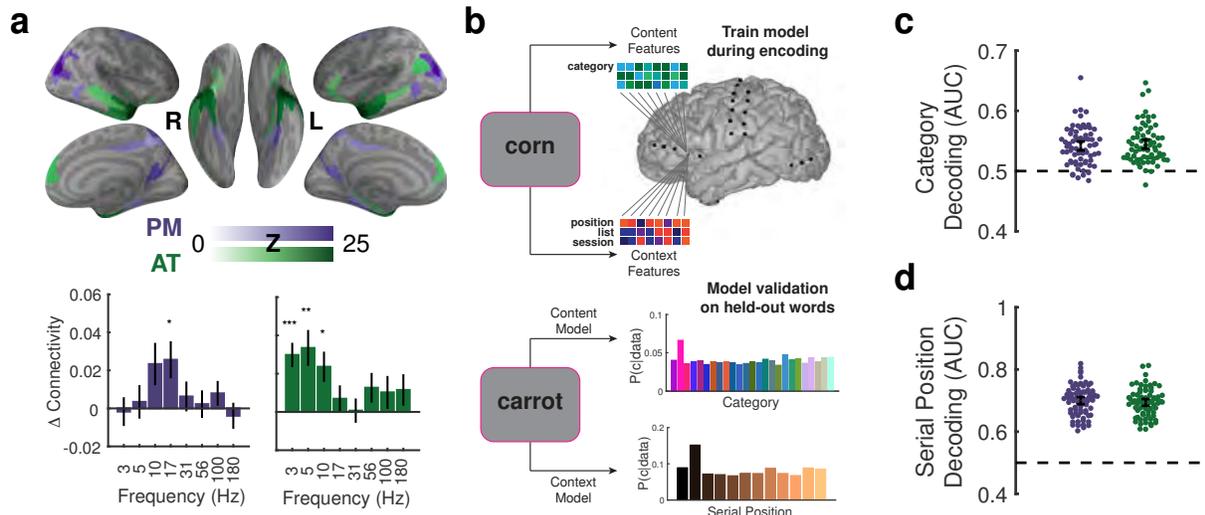


Figure 2 Network-based decoding of content and context. **a**, rsfMRI connectivity identifies distinct cortical networks. Top: Functional connectivity (Fisher Z) to cortical targets of the PM and AT networks. Bottom: difference in connectivity of recording sites within vs. between the two networks. Frequency specificity was observed within each network ($P < 0.05$, FWER corrected). **b**, Modeling schematic. Ridge regression modeled evoked neural activity during stimulus encoding. Models were validated by decoding the category and serial position of held out stimuli during encoding. **c**, Reliable category decoding in the PM (one tailed sign-test, $P < 0.0001$) and AT (one tailed sign-test, $P < 0.0001$) networks during encoding. **d**, Serial position decoding for the PM (one tailed sign-test, $P < 0.0001$) and AT (one tailed sign-test, $P < 0.0001$) networks during encoding. $N = 69$ subjects. All tests are two-tailed unless otherwise noted. Error bars denote ± 1 SEM * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$

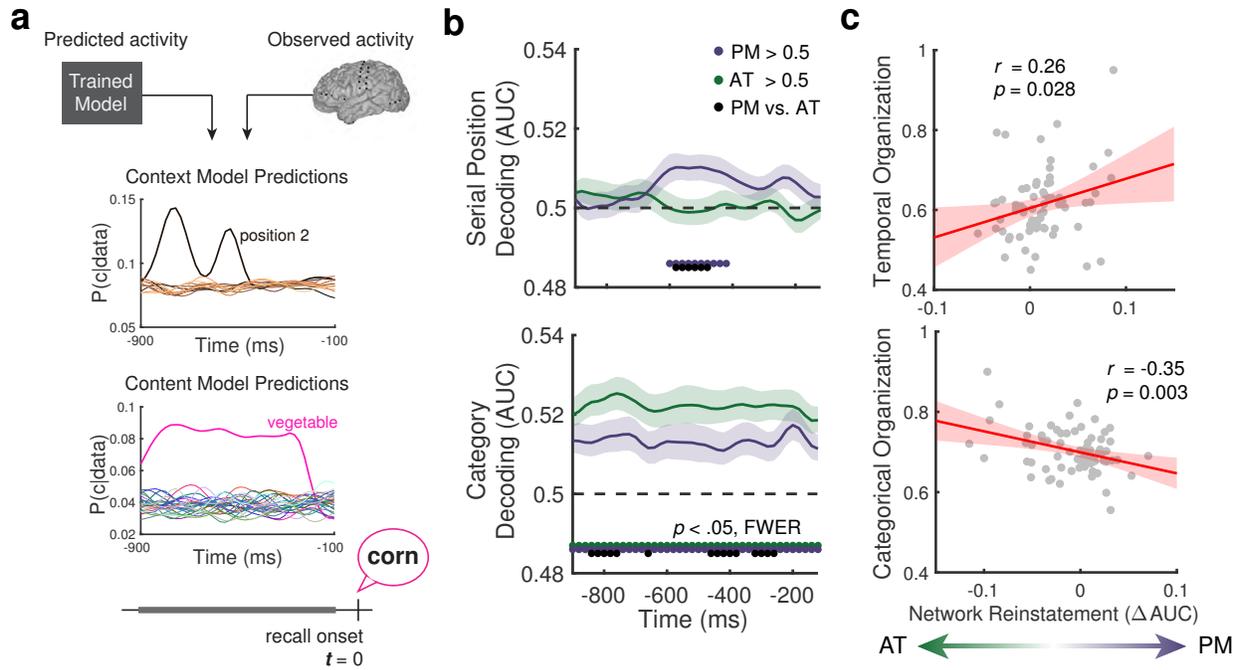


Figure 3 Reinstatement of content and context information during memory search. **a**, Simulated reinstatement analysis. Models trained during encoding predict the probability that each epoch precedes recall of an item from one of 12 serial positions (context model, top) or 25 categories (content model, bottom). **b**, Decoding the serial position (top) and semantic category (bottom) from reinstated patterns of neural activity within each network. **c**, Relationship between network reinstatement and organization of recall sequences along temporal and categorical dimensions. Shaded regions denote SEM across ($N = 69$) subjects.

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590 **Acknowledgments**

591 We thank Medtronic and Blackrock Microsystems for providing neural recording equipment. We also thank Drs. Ethan
592 Solomon and Nora Herweg for providing feedback on this work. This work was supported by the DARPA Restoring
593 Active Memory (RAM) program (Cooperative Agreement N66001-14-2-4032). We are indebted to all patients who
594 have selflessly volunteered their time to participate in our study. The views, opinions, and/or findings contained in
595 this material are those of the authors and should not be interpreted as representing the official views or policies of
596 the Department of Defense or the U.S. Government. Data were provided in part by the Human Connectome Project,
597 WU-Minn Consortium (Principal Investigators: David Van Essen and Kamil Ugurbil; 1U54MH091657) funded by
598 the 16 NIH Institutes and Centers that support the NIH Blueprint for Neuroscience Research; and by the McDonnell
599 Center for Systems Neuroscience at Washington University.

600 **Author Contributions**

601 M.J.K. and Y.E. designed the study; J.E.K. analyzed data and drafted the manuscript. J.E.K. and M.J.K. edited the
602 manuscript. J.M.S. performed anatomical localization of depth electrodes. M.R.S., G.W., B.L., R.G., B.C.J., K.A.Z.,
603 and S.A.S. recruited subjects and performed clinical duties associated with data collection.

604 **Competing Interests**

605 M.R.S. is the principal investigator (PI) of research contracts with SK Life Science, Takeda, UCB Pharma, Neurelis,
606 Eisai, Medtronic, Engage, and Cavion. M.R.S. serves as a consultant to Medtronic through Jefferson University which
607 receives all compensation for these services. B.C.J. has research contracts with Neuropace, Medtronic, Sunovion, and
608 Eisai. R.E.G. serves as a consultant to Medtronic, a subcontractor on the RAM project. R.E.G. receives compensation
609 for these services; the terms of this arrangement have been reviewed and approved by Emory University in accordance
610 with its conflict of interest policies. The remaining authors declare no competing interests.